IJPSR (2010), Vol. 1, Issue 5



Received 28 February, 2010; received in revised form 13 April, 2010; accepted 21 April, 2010

ONCE DAILY GASTRO RETENTIVE MUCOADHESIVE CEPHALEXIN MONOHYDRATE TABLET: FORMULATION AND *IN-VITRO* EVALUATION

K. G. Parthiban*, B. Senthil Kumar, R. Manivannan and D. Sanjeevi kumar

Department of Pharmaceutics, JKK Munirajah Medical Research Foundation, College of Pharmacy, Komarapalayam, Namakkal (DT), Tamil Nadu, India

ABSTRACT

Keywords:

Gastroretentive mucoadhesive tablet, Cephalexin monohydrate, controlled release, mucoadhesive strength, *in-vitro* release, stability study

Correspondence to author:

K. G. PARTHIBAN

JKKMMRF College of Pharmacy,

Komarapalayam, Namakkal (DT), Tamil Nadu, India

Email: manivannan_biotech@yahoo.co.in

Oral drug administration has been the predominant route for drug delivery due to the ease of administration, patient convenience and flexibility in formulations. Mucoadhesive tablets of Cephalexin monohydrate were prepared with an objective to increase the bioavailability by minimizing the first pass metabolism and also to reduce the frequency of administration. Carbopol 934p as a primary polymer and HPMC K15M, HPMC K4M, and HPMC K100M as secondary polymers in different proportions has been used to formulate the desired mucoadhesive formulation with other tablet excipients and lubricants to give good compressibility by dry granulation method. The tablets were characterized by weight variation, hardness, thickness, friability, swelling ability, dissolution profile, assay and mucoadhesive strength. The selected mucoadhesive formulation FC2 exhibited 99.51% of drug release in 24 hrs, the mucoadhesive strength was found to be 95.04 gm so it has enough strength to adhere on the mucosa for an extended period of time. Kinetic study has been studied for the selected formulation it follows zero order release and matches with Higuchi regression. Selected formulation FC2 showed no significant change in the physico chemical parameters after storage at 40°C±2 °C and 75% RH±5% for one month.

INTRODUCTION: Gastroretentive systems can remain in the gastric region for several hours and hence can significantly prolong the gastric residence time of drugs. Prolong gastric retention improves bioavailability, reduces drug wastage, and improves solubility for the drugs that are less soluble in the high pH environment of small intestine ¹. It has applications also for local drug delivery to the stomach and proximal small intestine. Therefore different approaches have been proposed to retain the dosage form in the stomach. Those approaches include synthesis of high density dosage form, flotation, sedimentation, expansion modified shape systems, comitent administration of drugs or excipients which slows the motility of stomach or small intestine, synthesis of bioadhesive or mucoadhesive dosage forms². Proximal small intestine (duodenum), the most effective strategy will be holding the formulation in the stomach³.

Mucoadhesion is the state in which two materials, at least one biological in nature, are held together for an extended period of time by interfacial forces. It is also defined as the ability of a material (synthetic or biological) to adhere to a biological tissue for an extended period of time ⁴. Cephalexin monohydrate is a semi synthetic antibiotic derived from cephalosporin 'C'. It is absorbed completely (80-100%) after oral administration and the protein binding of cephalexin is low (6-15%). The volume of distribution is 15 \pm 2.3 l. Cephalexin is not metabolized in the body and is excreted unchanged in the urine at

least two thirds by active secretion and having a biological half-life of 1 hr. To maintain therapeutic range, the drug should be administered 3—4 times a day, which leads to saw tooth kinetic and resulting in ineffective therapy. It treats most of the bacterial infections like otitis media, tonsils and adenoids, strep throat, laryngitis, acute bronchitis, urinary tract infection, pneumonia, jock itch, diverticulitis, impetigo, folliculitis ⁵.

The main objectives of the present work was to formulate cephalexin monohydrate mucoadhesive tablets by using Carbopol 934p as a primary polymer and HPMC K15M, HPMC K4M, and HPMC K100M as a secondary polymers in different proportions, with other tablet excipients and lubricants to give good compressibility by dry granulation method, which can provide constant effective drug release for 24 hours.

MATERIALS AND METHODS:

Materials: Cephalexin monohydrate were gift sample from Aurabindo pharma pvt ltd, HPMC K₄M were gift sample from Loba Chemie PVT Ltd, Mumbai, HPMC K₁₅M were gift sample from Reachem Laboratory chemical PVT Ltd, Chennai, HPMC K₁₀₀M were gift sample from Loba Chemie PVT Ltd, Mumbai. All other ingredients used were of analytical grade.

Method: Matrix type mucoadhesive tablets were prepared by dry granulation method. The mucoadhesive tablets were prepared by using Carbopol 934 (CP-934) as primary mucoadhesive polymer because of its excellent mucoadhesive properties. HPMC K_4M , HPMC $K_{15}M$ and HPMC $K_{100}M$ were used as secondary polymers. The effect of secondary polymer loading on drug release was studied. Carbopol 934p and secondary polymers in different concentrations were incorporated in different mucoadhesive tablets. The composition of different formulations is represented in table 1.

Procedure: The components of each formulation sufficient for 100 tablets were calculated and weighed except the lubricant, mixed and passed through the mesh (40μ) and triturated well in a glass mortar to ensure homogeneous mixing. Then this mass is compressed with more hardness with 12.5 mm round flat punches (slugging). Then these tablets are crushed and passed through 8 mm screen to form the granules, which is suitable for The lubricants compression. were weighed and mixed with the granules and compressed using 12×8 mm length die oblong punches on 16 station tablet compression machine (Cadmach Ahmadabad).

Physical characteristics of granules before compression: The flow angle of repose can be determined by fixed funnel method. The bulk density and tapped density were determined by the cylinder method. Compressibility index and hausner ratio was calculated by using following formula ^{6, 7, 8}.

Where V_0 = initial volume, Vf = tapped volume.

Determination of various physicochemical parameters for tablets: The weight variation can be tested by taking twenty tablets were weighed individually and the average weight was determined. The percentage deviation was calculated and checked for weight variation. The thickness of the 10 tablets of each formulation was measured using digital vernier calliper in mm. Hardness can be determined using a Monsanto hardness tester.

Pressure required to break the tablet is determined in kg/cm². Friability can be tested by taking 20 dedusted tablets and the percentage friability was calculated. The assay was carried out taking 20 tablets by liquid chromatographic method as per the specified monograph ⁹.

Swelling studies: The tablets of each formulation were weighed individually (designated as W_1) and placed separately in petri dishes containing water. At regular intervals (1, 2, 4, 8, 12, 16, 20, and 24 hr), the tablets were removed from the petri dishes and excess water was removed carefully by using filter paper ¹⁰. The swollen tablets were reweighed (W_2), the swelling index of each formulation was calculated using the formula,

 $W_1 - W_2$

 W_1

Compressibility index: =
$$100 \frac{(V_0 - Vf)}{V_0}$$
 Swelling Index (S.I) = Hausner Ratio: = $\frac{V_0}{Vf}$

INGREDIENTS (MG)	FA1	FA2	FA3	FB1	FB2	FB3	FC1	FC2	FC3
Cephalexin monohydrate	500	500	500	500	500	500	500	500	500
Carbopol 934P	400	400	400	400	400	400	400	400	400
HPMC K15M	225	250	275	-	-	-	-	-	
НРМС К4М	-	-	-	225	250	275	-	-	-
HPMC K100M	-	-	-	-	-	-	225	250	275
Magnesium stearate	10	10	10	10	10	10	10	10	10
Talc	10	10	10	10	10	10	10	10	10
Aerosil	15	15	15	15	15	15	15	15	15
Total	1160	1185	1210	1160	1185	1210	1160	1185	1210

TABLE 1: FORMULA OF CEPHALEXIN MONOHYDRATE MUCOADHESIVE TABLETS

In-vitro release studies: The release of Cephalexin monohydrate from mucoadhesive tablet was determined by using USP dissolution test apparatus II (paddle type). The whole assembly is kept in a jacketed vessel of water maintained at 37± 1⁰ C. Mucoadhesive tablet is stuck on to the bottom of the flask (so as to allow one sided release from the tablet). The beaker is filled with 900ml of water and maintained at 100 rpm. A sample of 3ml of the solution was withdrawn from the dissolution apparatus at 4 hour time intervals and filtered through Whattmann filter paper no: 42. It is replaced immediately with an equal amount of fresh water. The samples are then analyzed UV spectrophotometrically at 261 nm. Absorbance measured and % drug release was determined⁹.

Evaluation of Mucoadhesive Strength:

Detachment force measurement: This is the method used to measure *in-vitro* mucoadhesive capacity of different polymers. It is a modified method developed by Martti Marvola to assess the tendency of mucoadhesive materials to adhere to the oesophagus. The assembly of this apparatus consists of two glass slides; one modified physical balance, weights, thread, goat intestine, tyrode solution, distilled water and a beaker to hold the water ¹¹.

Method: Immediately after slaughter, the intestines was removed from the goat and transported to laboratory in tyrode solution is (g/litre); (sodium chloride 8 gm; potassium chloride 0.2 gm; calcium

 $2H_2O$ chloride 0.134 gm; sodium bicarbonate 1.0 gm; sodium dihydrogen phosphate 0.05 gm and glucose H₂O 1gm). During this experiment take the intestine in a specified area and place it on one glass slide and tie it. The glass slide with the intestine was affixed on one side floor below the modified physical balance. Already prepared 200 mg plain polymer tablet was pasted in another glass slide and it balanced in the assembled physical balance with a beaker in other side which is used to hold the water. Now the balance was calibrated.

Recording of Adherence: The plain polymer tablet in the slide was left on the intestine segment slide and lightly pressing the intestine segment with a forceps, the assembly should be kept undisturbed for a fixed time interval 5, 10, 15 and 30 minutes. Then water was added slowly in drop wise to the beaker aside. The amount of water required to pull out the tablet from the intestinal segment represents the force required to pull the tablet against the adhesion. The above same procedure is repeated for the comparative study between HPMC K₁₅M, HPMC K₄M, HPMC K₁₀₀M and Carbopol 934p. The force in Newton's is calculated by the equation,

F = 0.00981 W/2, Where W is the amount of water

Film Coating:

Preparation of coating solution:

1. Disperse HPMC 1.2 gm & Titanium dioxide 0.200 mg in Isopropyl Alcohol BP 12.1 ml and Methylene Chloride 39.2 ml.

2. Homogenize stage 1 for about 20 minutes.

Coating process:

- 1. Charge the whole batch into the coating pan. Check the rotating axis of the coating pan (10 to 15 rpm) blow the air at pressure of about 60 PSI. Switch ON the heaters of blower & allow the tablets to rotate. The temperature of the tablet bed should between 35° C to 40° C. start the coating process by spraying coating solution continuously.
- Continue the Process till the complete coating solution is consumed. Allow the tablets to cool to room temperature. Sprinkle Talcum BP quantity required on coated tablets & allow rotating tablets in coating pan for about 5 mins and unloading the tablets.

Kinetics of Drug Release: The order of rug release can be assessed by graphical treatment of drug release data. A plot of % drug remaining versus time would be linear if the drug release follows zero order (i.e. Concentration independent release)^[12]. A plot of log of % remaining drug versus time would be linear, if the drug release follows first order (i.e. concentration dependent release).

The linear equation for zero order drug release plot is:

$$C_t = C_0 - Kt$$

Where, C_t = Concentration remaining at time t, C_o = Original concentration, t = Time, K = Release rate.

The linear equation for first order release plot is;

$$\log C = \frac{\log C_0 K t}{2.303}$$

A matrix device as the name implies, consists of drug dispersed homogeneously throughout a polymer matrix. Mechanism of release from erodible matrix has been described by Hoffenberg. A simple expression describing release from erodible is,

$$\left(1 - \frac{Mt}{M}\right)^{1/3} = 1 - Kt$$

Where, Mt = mass of drug release at time t, M = mass release at the infinite time, K = rate of erosion, t = time

Thus a plot of $[1 - Mt / M]^{1/3}$ versus the time will be linear. If the release of drug from the matrix is erosion controlled. In order to ascertain whether the drug release occurs by diffusion or erosion, the drug release data was subjected to following modes of data treatments ¹³,

- 1. Amount of drug release versus square root of time (Higuchi Plot).
- 2. [1 Mt / M] ^{1/3} versus time (Hoffenberg).

Stability Study: Selected formulation FC2 was subjected to determine its shelf life i.e. stability study by using accelerated stability chamber, according to the WHO guidelines. The tablets were stored in the stability chamber under temperature 40° C $\pm 2^{\circ}$ C and 75% RH ± 5 % Relative humidity for one month. After the specified period the tablets are subjected to physical appearance, hardness, friability, dissolution and assay.

AND RESULTS **DISCUSSION:** Mucoadhesive Cephalexin tablets were prepared to increase the gastric retention of the dosage form so that they can be retained in the stomach for longer period of time and help in controlled release of drug up to 24hr. The mucoadhesive tablets were made using gel forming mucoadhesive such as Carbopol 934p, HPMC K₄M, HPMC K₁₅, and HPMC K₁₀₀M. To achieve the desired release the HPMC polymers (different grades) has been used in different proportions. Due to the changing the concentration of polymers the release rate will vary consequently. The granules ready for compression has been evaluated The prepared mucoadhesive tablets were evaluated thickness, weight variation, friability, hardness, in-vitro dissolution study, assay, study and mucoadhesive swelling strength.

Physio chemical characteristics of mucoadhesive tablets & granules: The prepared granules were evaluated and reported in the table 2. The flow property, bulk density and tapped density was found and the results are within the IP specification. The tablets were off-white oblong shaped concave appearance. The results of physiochemical characterisation of prepared tablets are shown table 3. The weight variation of all formulation was found to be within the range of -1.7 to +2.9%. The thickness of mucoadhesive tablets ranged between 8.97 to 9.18 mm. The hardness of the tablets was found in the range of 6.2 to 7.3 kg/cm². All tablets from all formulation showing satisfactory results as per Indian Pharmacopoeia.

Formulation code	Angle of Repose	Bulk Density	Tapped Density
F A1	19.77	0.698	0.832
F A2	20.01	0.712	0.887
F A3	20.54	0.724	0.921
F B1	19.35	0.696	0.856
F B2	22.86	0.758	0.974
F B3	21.53	0.774	0.981
FC1	21.37	0.725	0.945
F C2	22.53	0.710	0.924
FC3	23.32	0.689	0.861

TABLE 2: PHYSIO CHEMICAL EVALUATION OFPREPARED GRANULES

Swelling study: Swelling is also a vital factor to ensure the drug dissolution of the matrix tablet. The mucoadhesive tablet composed of polymeric materials build a gel layer around the tablet core when they come in contact with water. Table 4 shows the swelling index of all formulations. The mucoadhesive tablets containing Carbopol 934p and HPMC K15M showed higher swelling index in first two hours but could not maintain their matrix integrity up to 24 hr. The mucoadhesive tablets containing Carbopol 934p and HPMC K₄M showed higher swelling index in first two hours but could not maintain their matrix integrity up to 24 hr. The mucoadhesive tablets containing Carbopol 934p and HPMC K₁₀₀M showed constant increase in the swelling index up to 24hr. The initial swelling index was observed higher in all formulation due to the rapid hydration of HPMC graded polymers.

In- vitro release studies: The *in-vitro* release study of all formulations of mucoadhesive tablets was performed in water for 24 hours, and cumulative drug

release was calculated at four hour intervals. The results of in-vitro dissolution studies for all formulations are shown in the figure 1.The first three FA2, formulations FA1, FA3 were formulated by using drug with Carbopol 934p and HPMC K₁₅M. In this FA1 shows the drug release 97.79% in 14 hours and FA2, FA3 shows 99.51%, 95.82% in 16 respectively. Another hours three formulations FB1, FB2, FB3 were formulated by using drug with Carbopol 934p and HPMC K₄M. In this FB1 and FB2 shows the drug release 100.02% and 94.62% in 16 hours and, FB3 shows 99.65% in 18 hours. Last three formulations FC1, FC2, FC3 were formulated by using drug with Carbopol 934p and HPMC K₁₀₀M. In this FC1 shows the drug release 98.48% within 22 hours and FC2, FC3 shows 99.51%, 94.11% in 24 hours respectively. From this release study FC2 release the drug at predetermined and reproducible manner for 24 hours comparing to all other formulations and shows as best formulation.

From the above data we can conclude that drug combination with Carbopol 934p and HPMC K₁₅M release the drug quickly comparing to other formulation and Carbopol 934p and HPMC K₄M shows moderate release and Carbopol 934p and HPMC K_{100} combination is the best formulation. The mucoadhesive strength was found to be 95.04 gm, and from that concluded that the optimised formulation having enough mucoadhesive strength. The assay value for the selected formulation was found to be 99.01%, so it has within the limit of NLT 95% to NMT 102% as per IP.

EVALUATION	FORMULATION CODE								
PARAMETERS	FA1	FA2	FA3	FB1	FB2	FB3	FC1	FC2	FC3
Weight variation (%)	-1.9 to 2.1	-2.3 to 2.4	-2.2 to +1.7	-1.8 to +1.6	-1.7 to +2.7	-2.8 to +2.4	-2.1 to +2.9	-1.8 to +2.5	-2.9 to +2.3
Hardness kg/cm ²	6.5	7 .3	6.2	7	6.4	6	6.9	7.3	6.3
Thickness mm	8.97	9.01	9.12	8.90	8.99	9.03	8.95	9.09	9.18
Friability (%)	0.210	0.284	0.353	0.240	0.312	0.211	0.332	0.399	0.312

TABLE 4: SWELLING INDEX OF MUCOADHESIVE TABLETS

FORMULATION	SWELLING INDEX (MG)							
CODE	INITIAL	1 HOURS	4 HOURS	8 HOURS	12 HOURS	16 HOURS	20 HOURS	24 HOURS
FA1	1167	1755	1867	2015	2163	2311	2458	2599
FA2	1180	1826	1947	2102	2255	2413	2568	2725
FA3	1206	1862	1993	2154	2317	2482	2642	2801
FB1	1164	1765	1861	2016	2163	2314	2459	2605
FB2	1182	1787	1893	2038	2184	2328	2470	2617
FB3	1212	1824	1936	2084	2231	2383	2526	2680
FCI	1157	1783	1898	2053	2203	2355	2511	2666
FC2	1187	1811	1934	2089	2243	2394	2538	2693
FC3	1215	1851	1977	2136	2285	2443	2604	2752



Fig. 1: In-vitro release profile of all formulation

The results obtained for the selected formulation FC2 after the stability one month was listed in table 5. The tablets

does not showing any significant differences in physical appearance, friability, hardness, dissolution characteristics and assay. So the selected formulation is stable under the prescribed condition for one month.

Parameters	Results			
Description	No change.			
Friability Hardness	0.401% w/w 7.08 kg/cm ²			
Dissolution	98.78%			
Assay	98.12%			

Kinetics of Drug Release: The data obtained from in-vitro dissolution studies were fitted to zero order, first order, Higuchi, and Hoffenberg equations to confirm the order of the release. The data obtained from the calculations are shown in the table 6. From this data the drug release followed zero order release kinetics and it follows the diffusion mechanism for drug release. The FC2 formulation follows Zero order drug release (0.996) as well as diffusion (Higuchi) mechanism to release the drug from the formulation (0.946).

thickness, friability and weight variation. Formulation FC2 (Carbopol 934p&HPMC K100M) satisfies the in-vitro drug release up to 24 assay value also satisfies the IP limit and considered as the best formulation comparing to all other formulations. Mucoadhesive strength was studied for the selected formulation and it shows high mucoadhesive strength and Stability study was passed as per specification. The selected formulation follows the zero order release and exhibited diffusion dominated drug release. Further *in-vivo* and continuation of stability study are recommended.

Time (hr)	(Time) ^{1/2}	Cumulative % release	Amount of drug release	% of drug remained	Log % of drug remained	$\left(1-\frac{M_t}{M}\right)^{1/3}$
1	1.4142	5.05	25.28	94.95	1.9774	0.982854
4	2	20.74	103.71	79.26	1.8990	0.925439
8	2.8284	37.11	185.57	62.89	1.7985	0.856744
12	3.4641	54.08	270.42	45.92	1.6620	0.771474
14	3.7416	63.59	317.99	36.41	1.5612	0.714017
16	4	71.14	355.71	28.86	1.4602	0.660828
18	4.2426	79.79	398.99	20.21	1.3055	0.586766
20	4.4721	86.91	434.57	13.09	1.11694	0.507694
22	4.6904	93.85	469.28	6.15	0.788875	0.394594
24	4.8989	99.51	497.57	0.49	-0.3098	0.169386

TABLE 6: KINETIC OF RELEASE STUDY OF FC2

CONCLUSION: From the obtained results it can be concluded that all the formulations satisfy the official limits for preformulation study, hardness,

ACKNOWLEDGEMENT: We the authors are very much thankful to Dr. JKK Munirajah, M. Tech (Bolton), D. Litt, Managing Director, JKKM Group of Institutions for his support and 6. encouragement. Authors are also thankful to M/S Elegant drugs private Ltd., Hubli for providing all facilities to complete the research work.

REFERENCES:

- 1. Ponchel G and Irache JM: Specific and non specific bio adhesive particulate system for oral delivery to the GI tract. Advances in drug delivery 1998; Rev.34:191-219.
- 2. AkiyamaY, Nagahara N, Nara E, Yamamoto I, Azuma J, and Ogawa Y: Evaluation of Mucoadheesive microspheres in man on the basis the pharmacokinetics of furosemide and riboflavin, compounds with limited gastrointestinal absorption sites J.Pharm. Pharmacol 1998; 50: 159-166.
- 3. Chen J, Blevins WE, Park H and Park K: Gastric retention properties of superporous hydrogen composites. J.Controlled Release: 2000; 64: 159-166.
- 4. Vyas SP and RP Khar: Controlled drug delivery systems, Concepts and advances, first edition 2002; 257-295.
- 5. Shin SC and Cho SJ: Drug Dev. Ind. Pharm 1996; 22:299-305.

- Cooper J and Gunn C: Tutorial Pharmacy, Powder flow and compaction, New Delhi, India: CBS Publishers and Distributors; 1986:211-233.
- Shah.D, Shah Y,Rampradhan M, Development and evaluation of controlled release diltiazem hydrochloride Micro particles using cross-linked poly(vinyl alcohol). Drug Dev Ind Pharm. 1997; 23(6):567-574.
- Aulton ME, Wells TI Pharmaceutics. The science of Dosage form Design. London, England: Churchil Livingstone; 1988.
- 9. Pharmacopoeia of India. New Delhi: Ministry of Health and Family Welfare, Government of India, Controller of Publications 2007: Vol 1; 182-183., Vol 2; 889.
- 10. Senapathi MK, Srinatha A, Pandit JK, Invitro Release Characteristics of Matrix Tablets: Study of Karaya gum and Guar gum as the release Modulators. International Journal of Pharmaceutical Sciences 2006; 68: 824-826.
- Madhusudan Rao Y, Vani G and Balaramesh achary R: Design and evaluation of mucoadhesie drug delivery systems, Indian drugs 1999; 35:558-565.
- 12. Alfred Martin and James Swarbrick: Physical Pharmacy 3rd edition 1994: 352-362
- 13. Higuchi T: Mechanism of sustained action medication. Theoretical analysis of rate release of solid drugs dispersed in solid matrices. J Pharm Sci.1963; 52:1145-1149.