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FORMULATION AND *IN-VITRO* EVALUATION OF FLOATING EFFERVESCENT TABLETS OF RANITIDINE HYDROCHLORIDE

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Keywords:

Ranitidine hydrochloride, Hydroxy propyl methyl cellulose (HPMC), Xanthan gum, Guar gum and Floating Effervescent matrix tablets.

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ABSTRACT: The main objective of the present work is to develop Floating Effervescent matrix tablets of Ranitidine hydrochloride using different polymers viz. hydroxy propyl methyl cellulose (HPMC), Xanthan gum and Guar gum. Varying ratios of drug and polymer like 1:0.6 and 1:1 were selected for the study. After fixing the ratio of drug and polymer for control the release of drug up to desired time, the release rates were modulated by combination of two different rate controlling material. After evaluation of physical properties of tablet, *in-vitro* buoyancy studies, Swelling index and *in vitro* release study were performed in 0.1N Hcl up to 12 hrs. Dissolution data was analyzed by Korsmeyer-Peppas power law expression and modified power law expression. It was observed that matrix tablets contained polymer blend of HPMC K100M/Guar gum were successfully sustained the release of drug upto 12 hrs. Among all the formulations, formulation F9 which contains 50% HPMC K100M and 50% of Guar gum has released the drug which follow Zero order kinetics via, swelling, diffusion and erosion. The release profile of formulation F9 was comparable with the marketed product. The FTIR study revealed that there was no chemical interaction between drug and excipients.

INTRODUCTION: The oral route is considered as the most promising route of drug delivery. Effective oral drug delivery may depend upon the factors such as gastric emptying process, gastrointestinal transit time of dosage form, drug release from the dosage form and site of absorption of drugs. Most of the oral dosage forms possess several physiological limitations such as variable gastrointestinal transit, because of variable gastric emptying leading to non-uniform absorption profiles, incomplete drug release and shorter residence time of the dosage form in the stomach.

This leads to incomplete absorption of drugs having absorption window especially in the upper part of the small intestine, as once the drug passes down the absorption site, the remaining quantity goes unabsorbed. The gastric emptying of dosage forms in humans is affected by several factors because of which wide inter- and intra-subject variations are observed¹⁻⁶. Since many drugs are well absorbed in the upper part of the gastrointestinal tract, such high variability may lead to non-uniform absorption and makes the bioavailability unpredictable. Hence a beneficial delivery system would be one which possesses the ability to control and prolong the gastric emptying time and can deliver drugs in higher concentrations to the absorption site (i.e. upper part of the small intestine).

The identification of new diseases and the resistance shown towards the existing drugs called

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for the introduction of new therapeutic molecules. In response, a large number of chemical entities have been introduced, of which some have absorption all over the gastrointestinal tract (GIT), some have absorption windows (i.e. absorption sites, especially the upper part of the small intestine) and some drugs have poor solubility in intestinal media. The drugs belonging to the second and third categories, and the drugs which are required for local action in the stomach, require a specialized delivery system. All the above requirements can be met and effective delivery of the drugs to the absorption window, for local action and for the treatment of gastric disorders such as gastro-esophageal reflux, can be achieved by floating drug delivery systems (FDDS).⁷⁻¹²

To date, a number of FDDS involving various technologies, carrying their own advantages and limitations were developed such as, single and multiple unit hydro dynamically balanced systems (HBS), single and multiple unit gas generating systems, hollow microspheres and raft forming systems¹²⁻¹⁷.

The hydrodynamic balanced system (HBS) also called Floating drug delivery system (FDDS) is an oral dosage form (capsule or tablet) designed to prolong the residence time of the dosage form within the GIT. It is a formulation of a drug with gel forming hydrocolloids meant to remain buoyant in the stomach contents. Drug dissolution and release from the dosage form retained in the stomach fluids occur at the pH of the stomach under fairly controlled conditions³. The retentive characteristics of the dosage form are not significant for the drugs that:

1. Are insoluble in intestinal fluids
2. Act locally
3. Exhibit site-specific absorption.

However, the system can be used for most of the drugs where controlled (sustained) release of the dosage form is desired by the oral route.

The formulation of the dosage form must comply with three major criteria for HBS.

It must have sufficient structure to form a cohesive gel barrier.

It must maintain an overall specific gravity less than that of gastric content.

It should dissolve slowly enough to serve as a "Reservoir" for the delivery system.¹⁸⁻²²

Drug Profile:

Name: Ranitidine hydrochloride.

ii. Type: A non-imidazole blocker of those histamine receptors that mediate gastric secretion (H₂ receptors). It is used to treat gastrointestinal ulcers.

iii. Structure:

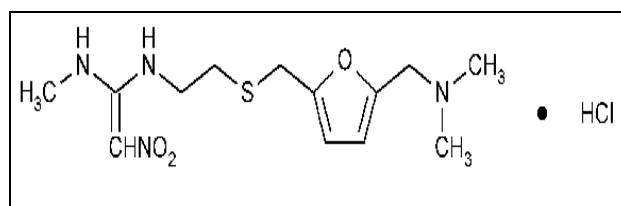


FIG.1: STRUCTURE OF RANITIDINE

iv. Categories:

Anti-Ulcer Agents, Histamine H₂ Antagonists

v. Chemical Formula: C₁₃H₂₂N₄O₃S

vi. IUPAC Name:

dimethyl [(5-[[[(E)-1-(methylamino)-2-nitroethenyl] amino] ethyl] sulfanyl] methyl] furan-2-yl) methyl]amine.

MATERIALS AND METHODS:

TABLE 1: MATERIALS USED IN THE STUDY

S.No	Active and inactive pharmaceutical ingredients	Suppliers
1	Ranitidine Hydrochloride	Zhaveri Pharmakem, Mumbai
2	Guar gum	FMC Biopolymer, USA
3	Xanthan gum	Aqualon, USA
4	Sodium bicarbonate	Colorcon, Goa
5	Mannitol	DOW, USA
6	Hydroxyl propyl methyl cellulose (HPMC K100M)	Colorcon Asia Pvt. Ltd., Goa
7	Hydroxyl propyl methyl cellulose	Colorcon Asia Pvt. Ltd., Goa

	(HPMC K4M)	
8	Magnesium Stearate	LobaChemie
9	Talc	LobaChemie
10	Isopropyl alcohol	Colorcon , Goa
11	Dicalcium phosphate	Colorcon , Goa

- The solutions were analyzed spectrophotometrically at 314nm using UV visible spectrophotometer.

Preparation of standard solution of Ranitidine hydrochloride:

Stock solution: 100mg of Ranitidine HCl was weighed accurately and transferred into a 100 ml volumetric flask. Then the volume was made upto 100ml using water.

Standard solution: 10ml of solution was withdrawn from the above stock solution and then made upto 100ml in another 100ml volumetric flask and this solution is considered as standard solution (100µg/ml).

- From the above standard solution 0.5, 1, 1.5, 2, 2.5ml was withdrawn and diluted to 10ml to get 5, 10, 15, 20, 25µg/ml concentration.

Standard Calibration Curve:

TABLE 2: STANDARD CALIBRATION CURVE

S.No	Concentration (µg/ml)	UV Absorbance at 226 nm
1	0 µg/ml	0.00
2	5µg/ml	0.183±0.02
3	10µg/ml	0.358±0.02
4	15µg/ml	0.536±0.02
5	20µg/ml	0.710±0.02
6	25µg/ml	0.891±0.02

Formulation development:

Preparation of matrix tablets by wet granulation method: Different tablet formulations were prepared by wet granulation method.

Formulation table:

TABLE 1: FORMULATION TABLE

Ingredients(mg)	F1	F2	F3	F4	F5	F76	F7	F8
API	150	150	150	150	150	150	150	150
HPMC K100M	100	-	-	-	150	-	-	-
Guar gum	-	100	-	-	-	150	-	-
HPMC K4M	-	-	100	-	-	-	150	-
Xanthum gum	-	-	-	100	-	-	-	150
Magnesium Stearate	3	3	3	3	3	3	3	3
Sodium bicarbonate	50	50	50	50	50	50	50	50
Talc	2	2	2	2	2	2	2	2
Mannitol	85	85	85	85	35	35	35	35
Isopropyl alcohol	2	2	2	2	2	2	2	2
Dicalcium phosphate	8	8	8	8	8	8	8	8
Total	400	400	400	400	400	400	400	400

TABLE 2: FORMULATION TABLE

Ingredients(mg)	F9	F10	F11	F12	F13	F14
API	150	150	150	150	150	150
HPMC K100M	50	50	50	-	-	-
Guar gum	50	-	-	50	50	-
HPMC K4M	-	50	-	50	-	50
Xanthum gum	-	-	50	-	50	50
Magnesium Stearate	3	3	3	3	3	3
Sodium bicarbonate	50	50	50	50	50	50
Talc	2	2	2	2	2	2
Mannitol	85	85	85	85	85	85
Isopropyl alcohol	2	2	2	2	2	2
Dicalcium phosphate	8	8	8	8	8	8
Total	400	400	400	400	400	400

Drug and excipient compatability studies by FTIR: The compatibility between the drug and polymer was evaluated by peak matching method.

There was no appearance or disappearance of the drug polymer mixture, which confirmed the

absence of any chemical interactions between the drug and polymer.

Evaluation of Precompression Blend:

a) Particle size distribution: 10.35 grams of sample was taken and added to an assembly of sieves consisting ASTM sieve numbers # 30, 40, 60, 80, 100, 120 base. Then assembly was closed and kept on sieve shaker and started analysis. Weights retained were checked for every 5 minutes and process was continued until variation in weights retained was not more than 5% or 0.1 gram. 20 minutes was set as end point based on the observation. Calculations were made to obtain cumulative percentage weight retained.

b) Angle of Repose:

The angle of repose of granules was determined by the funnel-method. The granules were allowed to flow through the funnel freely onto the surface. The diameter of the powder cone measured and angle of repose was calculated using the following equation.

$$\tan \theta = h/r$$

Where, h and r are the height and radius of the powder cone, θ is the angle of repose.

c) Determination of Bulk Density and Tapped Density:

The density apparatus was set for 100 tabs and after that the volume (V_f) was measured and continued operation till the two consecutive readings were equal. The bulk density and the tapped density were calculated using the following formulae.

$$\text{Bulk density} = W/V_0$$

$$\text{Tapped density} = W/V_f$$

Where, W= Weight of the powder

V_0 = Initial volume

V_f = final volume

d) Compressibility Index (Carr's Index):

Carr's index (CI) is an important measure that can be obtained from the bulk and tapped densities. In theory, the less compressible a material the more flowable it is

$$CI = (TD-BD) \times 100/TD$$

where, TD is the tapped density and BD is the bulk density.

e) Hausner's Ratio:

It is the ratio of tapped density and bulk density. Hausner found that this ratio was related to interparticle friction and, as such, could be used to predict powder flow properties (Lachman et al., 1987).

Evaluation of Matrix Tablets:

a) Thickness:

Twenty tablets from the representative sample were randomly taken and individual tablet thickness was measured by using digital vernier caliper. Average thickness and standard deviation values were calculated.

b) Hardness:

Tablet hardness was measured by using Monsanto hardness tester. From each batch six tablets were measured for the hardness and average of six values was noted along with standard deviations.

c) Friability Test:

From each batch, ten tablets were accurately weighed and placed in the friability test apparatus (Roche friabilator) at 25 rpm/min for 4 min.

d) Weight Variation Test:

To study weight variation individual weights (W_i) of 20 tablets from each formulation were noted using electronic balance. Their average weight (W_A) was calculated.

e) Drug Content (Assay):

Ten tablets were weighed and taken into a mortar and crushed into fine powder. An accurately weighed portion of the powder equivalent to about 100 mg of TM was transferred to a 100 mL volumetric flask containing 70 mL of 0.1N HCl. It was shaken by mechanical means for 1h. Then it was filtered through a Whatman filter paper (No. 1) and diluted to 100 mL with 0.1N HCl. From this resulted solution 1 mL was taken, diluted to 50 mL with 0.1N HCl and absorbance was measured against blank at 314 nm.

f) Swelling Index of Formulation:

The swelling behaviour of floating tablets was measured by studying its weight gain (or) water uptake, water uptake was measured in terms of percent weight gain was given by equation.

$$WU = (W1 - W0) \times 100 / W0$$

g) In-vitro Buoyancy Studies:

The tablet were placed in a beaker containing 0.1N Hcl. The time required for the tablet to rise to the surface and float was determined as floating lag time. The total time for the tablet remain buoyant reported as floating time.

h) In -vitro drug release characteristics:

Drug release was assessed by dissolution test under the following conditions:

n = 3, USP type II dissolution apparatus (paddle method) at 100 rpm in 900 mL of 0.1N HCl for first 2 hours and the phosphate buffer pH 6.8 from 3 to 12 hours, maintained at 37°C±0.5°C. An aliquot (5mL) was withdrawn at specific time intervals and replaced with the same volume of prewarmed (37°C±0.5°C) fresh dissolution medium. The samples withdrawn were filtered through Whatman filter paper (No.1) and drug content in each sample was analyzed by UV-visible spectrophotometer at 314 nm.

RESULTS:

Standard Calibration Graph of Ranitidine Hydrochloride:

TABLE 4: CALIBRATION GRAPH

S.No	Concentration µg/ml	UV Absorbance at 314 nm
1	0	0.00
2	5	0.183±0.02
3	10	0.358±0.02
4	15	0.536±0.02
5	20	0.710±0.02
6	25	0.891±0.02

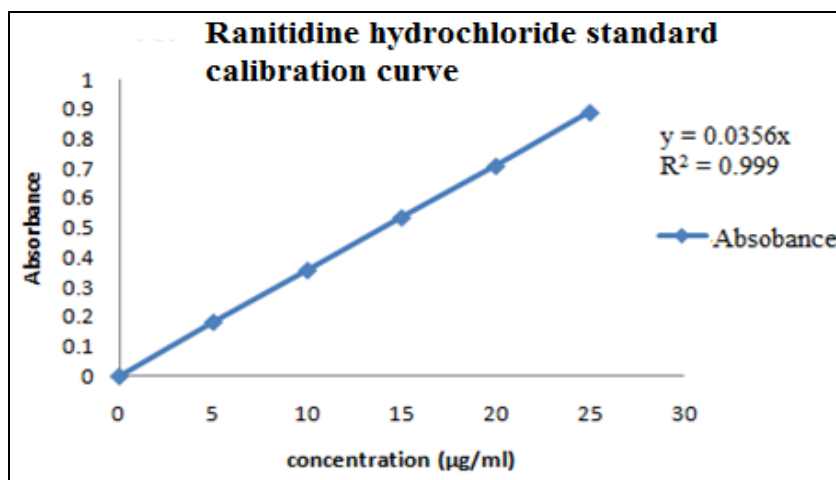


FIG.2: STANDARD CALIBRATION CURVE OF RANITIDINE HYDROCHLORIDE

Particle size distribution of drug:

TABLE 5: PARTICLE SIZE DISTRIBUTION OF DRUG

Sieve Mesh Number	Sieve Size Opening µm	Mass of Sample Retained On Each Sieve(g)	Percentage of Sample Retained on Each Sieve (%)	Cumulative Percentage Of Sample Retained on Each Sieve (%)
30	841	0.08	0.772947	0.8
40	425	0.06	0.57971	1.4
60	250	0.05	0.483092	1.9
80	180	0.41	3.961353	5.9
100	150	1.55	14.97585	20.9
120	130	2.62	25.31401	46.2
Pan	-	5.55	53.62319	99.8

It was observed from table that from percentage cumulative size distribution it was found that around 2% of particles were above 250 microns and 98% were below 250 microns.

Drug-excipient compatability by FTIR studies:

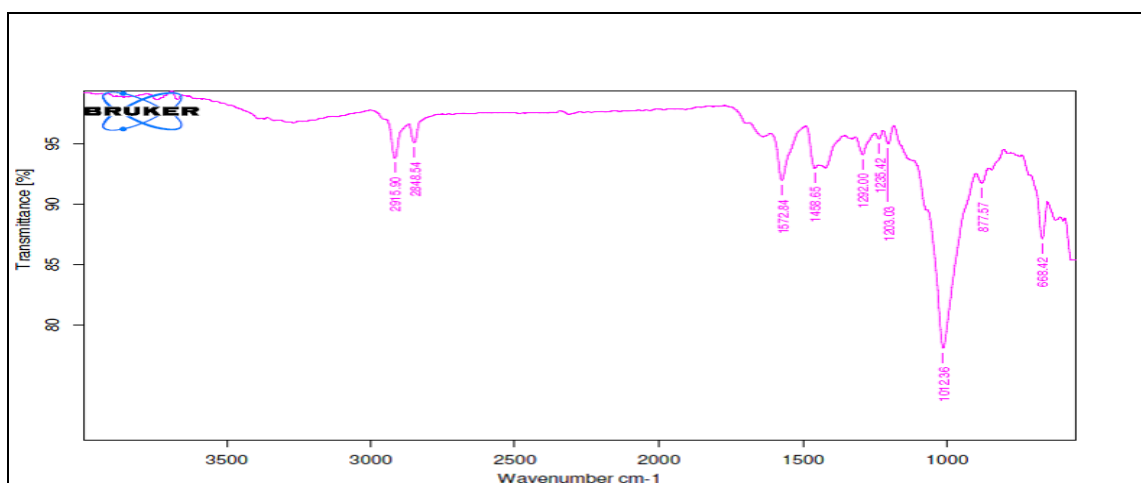


FIG.3: RANITIDINE WITH EXCIPIENTS DRUG AND POLYMER

Characterization wet granulation blend:

TABLE 6: CHARACTERIZATION WET GRANULATION BLEND.

Formulations	Angle of repose (°)	Bulk Density (g/mL)	Tapped Density (g/mL)	Carr's Index (%)	Hausner's ratio
F1	25.49	0.214	0.251	14.74	1.17
F2	26.24	0.308	0.364	16.07	1.18
F3	29.05	0.276	0.322	14.28	1.16
F4	26.97	0.341	0.388	12.11	1.13
F5	29.25	0.324	0.376	13.82	1.16
F6	32.27	0.320	0.397	19.39	1.24
F7	33.65	0.521	0.629	21.5	1.20
F8	33.21	0.518	0.627	26.38	1.21
F9	26.56	0.422	0.506	15.38	1.19
F10	28.75	0.481	0.572	15.90	1.18
F11	27.33	0.475	0.566	16.07	1.19
F12	26.27	0.487	0.561	13.19	1.15
F13	26.43	0.412	0.483	22.45	1.17
F14	24.77	0.488	0.537	9.12	1.10

It was observed from the table that the formulation:

F1, F2, F3, F4, F5, F9, showed excellent flow properties and formulations F6, F7, F8 showed good flow properties and formulations F10, F11, F12, F13, 14 showed passable flow properties. Formulations F1, F3, F4, F5, F6, F10, F11 showed fair compressibility index and formulation F9 showed good compressibility index and formulation F8 showed poor compressibility index, formulations F7, F13 showed passable compressibility index. This outcome may be due to the use of lubricants or may be due to the method adopted.

Characterization of tablets prepaed by wet granulation:

It was observed from the table that the variation in weight was within the range of ± 7.5% complying with USP pharmacopoeial specifications. The thickness of tablets was found to be between 2.81-3.84 mm. The hardness for all formulations was found to be between 5-6 kp. The friability was below 0.8% for all the formulations. The percentage drug content varied between 99.4-100.6 in different formulations indicating uniformity in the drug distribution among the tablets.

TABLE 7: CHARACTERIZATION OF TABLETS PREPAED BY WET GRANULATION

F.Code	Hardness (kg/cm ²) †	Thickness (mm) ‡	Weight (mg) ‡	Friability (%)	Drug content * (%)
F1	5.50 ±0.44	3.22±0.17	229.8±1.48	0.48	98.25±1.37
F2	5.70±0.31	3.37±0.25	200.4±0.54	0.42	95.28±0.80
F3	6.20±0.40	3.14±0.80	228.6±0.41	0.28	99.12±2.47
F4	5.3 ±0.55	3.20±0.20	228.8±1.64	0.52	97.35±0.43
F5	5.50±0.57	3.08±0.66	325.6±1.14	0.56	95.28±0.80
F6	5.50±0.30	3.33±0.25	324.2±0.83	0.58	99.53±1.87
F7	5.90±0.57	3.24±0.71	324.9±0.67	0.47	93.28±1.99
F8	5.60±0.60	3.32±0.89	324.0±0.43	0.39	95.35±1.14
F9	5.50±0.60	3.38±0.73	325.5±0.80	0.56	100.24±1.25
F10	6.10±0.31	3.00±0.68	324.2±0.83	0.42	91.29±0.98
F11	6.30±0.37	2.98±0.88	326.1±0.93	0.48	97.35±0.43
F12	5.90±0.65	3.33±0.59	325.8±0.38	0.37	98.90±2.31
F13	6.00±0.50	3.06±0.46	324.2±0.83	0.29	94.57±1.22
F14	5.90±0.57	2.98±0.38	327.2±0.92	0.35	90.35±2.09

Dissolution studies:

TABLE 8: DISSOLUTION STUDIES OF MARKETED PRODUCT (ZANTAC150mg)

Sampling Time (hr)	Cumulative % Drug Release
0	0
0.25	12.5
0.5	22.84
1	34.23
2	41.94
4	54.36
6	68.89
8	82.3
10	88.96
12	96.45

Post compression tests of marketed product Zantac (150mg):

TABLE 9: POST COMPRESSION TESTS

Hardness (kg/cm ²)	Thickness(mm)	Weight(mg)	Friability (%)
3.37 ± 0.74	3.20 ± 0.20	127 ± 0.83	0.56

In-vitro dissolution profile for the formulation F1, F2, F3 and F4:

TABLE 10: IN- VITRO DISSOLUTION PROFILE FOR THE FORMULATION F1, F2, F3 AND F4

Time in Hours	% cumulative Drug Release			
	F1	F2	F3	F4
0	0	0	0	0
0.25	8.25	18.32	28.52	16.32
0.5	14.32	25.46	39.42	23.89
1	23.96	32.83	54.52	30.42
2	31.8	48.23	73.14	41.96
4	39.43	65.43	89.76	69.76
6	42.54	83.72	101.32	87.42
8	57.85	99.83	-	99.97
10	61.23	-	-	-
12	72.85	-	-	-

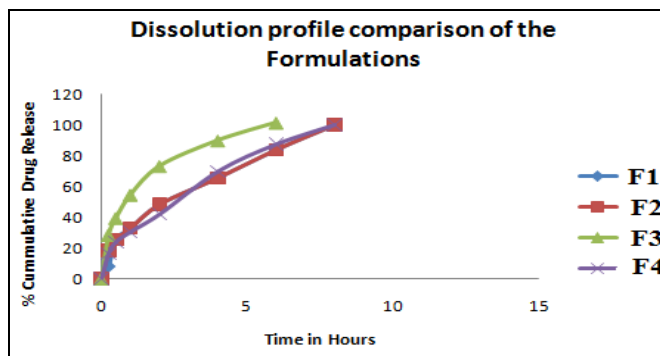


FIG.4: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F1, F2, F3 AND F4

TABLE: 11. IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F5, F6, F7 AND F8

Time in Hours	% cumulative Drug Release			
	F5	F6	F7	F8
0	0	0	0	0
0.25	10.35	17.52	27.32	16.36
0.5	19.76	23.52	34.97	21.93
1	27.42	30.72	47.52	28.27
2	36.93	44.92	69.38	43.6
4	49.16	59.76	81.96	55.46
6	67.23	78.13	103.72	71.2
8	75.42	91.6	-	93.86
10	79.73	99.72	-	100.83
12	84.72	-	-	-

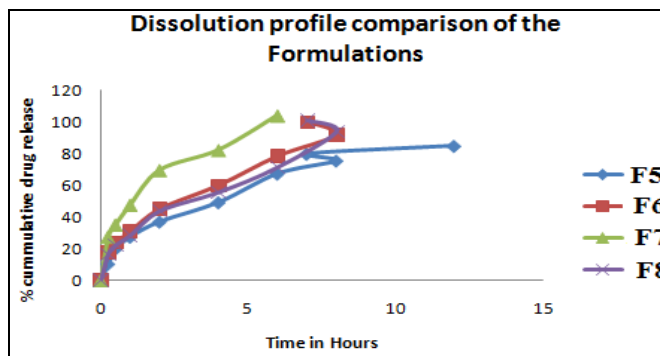


FIG.5: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F5, F6, F7 AND F8

In-vitro dissolution profile for the formulation F9, F10, F11 and F12:

TABLE 12: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F9, F10, F11 AND F12

Time in Hours	% cumulative Drug Release			
	F9	F10	F11	F12
0	0	0	0	0
0.25	13.72	17.32	12.23	14.92
0.5	23.72	25.42	19.72	17.33
1	36.23	33.27	34.89	22.86
2	45.36	45.86	41.76	40.72
4	58.96	62.36	59.6	61.56
6	72.53	73.15	77.42	68.96
8	85.16	81.28	85.42	90.2
10	92.16	87.69	89.23	104.7
12	99.8	91.23	93.76	-

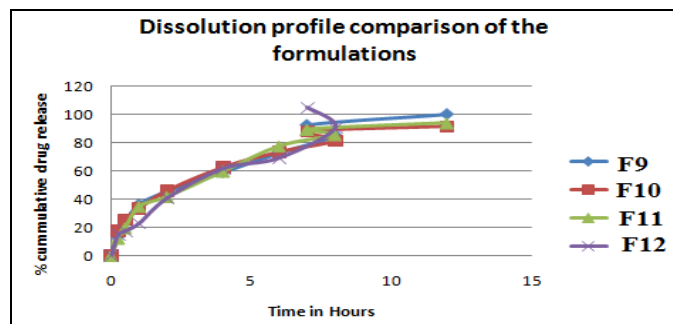


FIG.6: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F9, F10, F11 AND F12

In-vitro dissolution profile for the formulation F13 and F14

TABLE 13: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F13 AND F14

Time in Hours	% Cumulative Drug Release	
	F13	F14
0	0	0
0.25	19.32	15.42
0.5	27.48	18.32
1	32.89	24.72
2	41.72	38.92
4	49.38	52.72
6	52.73	66.23
8	58.42	71.32
10	63.23	101.32
12	69.72	-

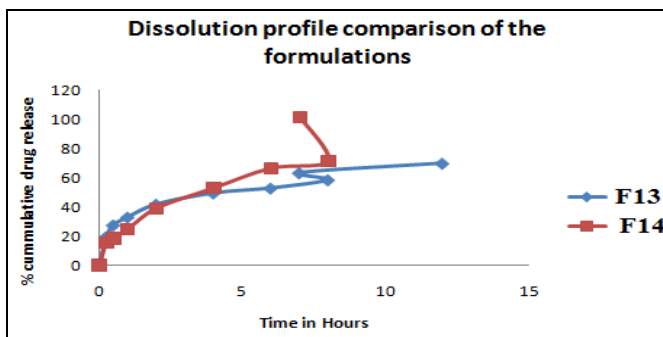


FIG.7: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION F13 AND F14

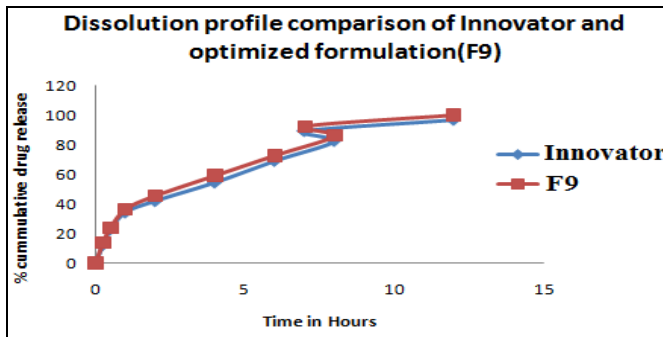
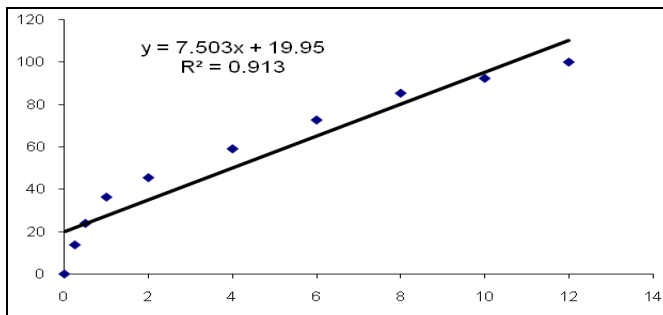


FIG.8: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION INNOVATOR AND OPTIMIZED FORMULATION (F9)

Release Kinetics:

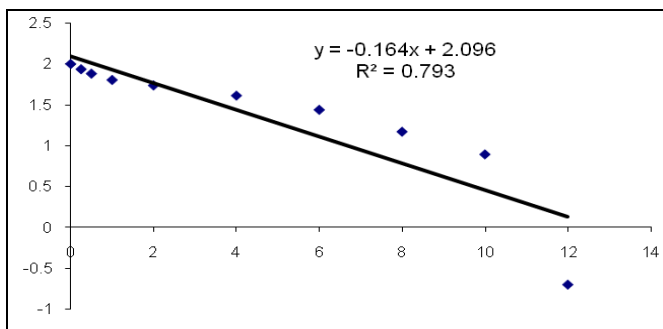
Zero order:



x-axis-time (hrs)
y-axis-cumulative percentage drug release

FIG.9: ZERO ORDER

First order:



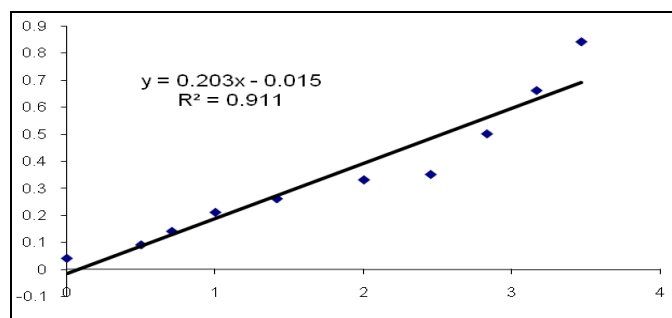
x-axis-time(hrs)
y-axis-log cumulative percentage drug remaining

FIG.10: FIRST ORDER

In-vitro dissolution profile for the formulation innovator and optimized formulation (F9):

TABLE 14: IN-VITRO DISSOLUTION PROFILE FOR THE FORMULATION INNOVATOR AND OPTIMIZED FORMULATION (F9)

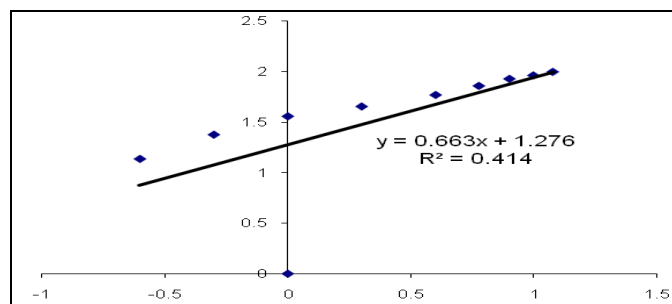
Time in Hours	% Cumulative Drug Release	
	Innovator	F9
0	0	0
0.25	12.5	13.72
0.5	22.84	23.72
1	34.23	36.23
2	41.93	45.36
4	54.36	58.96
6	68.89	72.53
8	82.3	85.16
10	88.96	92.16
12	96.45	99.8



x-axis-square root of time
y-axis-cumulative percentage drug release.

FIG.11: HIGUCHI

Korsemeyer and pappas:



x-axis-log time
y-axis-log cumulative percentage drug release.

FIG.12: KORSEMEYER AND PAPPAS

In-vitro buoyancy:

TABLE 15: IN-VITRO BUOYANCY

Formulation Batch	Buoyancy in Minutes
F1	10
F2	15
F3	30
F4	45
F5	85
F6	100
F7	110
F8	140
F9	655
F10	470
F11	490
F12	370
F13	310
F14	455

Swelling Index:

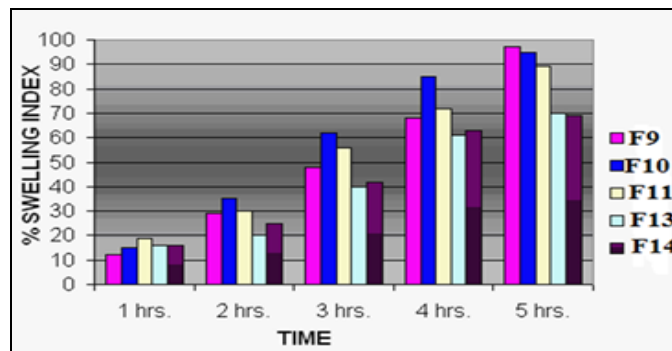


FIG.13: SWELLING INDEX

Similarity factor:

Similarity and difference factor

TABLE 16: SIMILARITY AND DIFFERENCE FACTOR

Time (t) [in Hours]	Innovator	Test (T)	Rt-Tt	(Rt-Tt) ²	Rt-Tt
0	0.00	0.00	0.00	0.00	0.00
1	24	25	-1.00	1.00	1.00
2	33	35	-2.00	4.00	2.00
3	49	51	-2.00	4.00	2.00
4	59	62	-3.00	9.00	3.00
6	70	73	-3.00	9.00	3.00
8	79	81	-2.00	4.00	2.00
10	84	87	-3.00	9.00	3.00
12	95	97	-2.00	4.00	2.00
Sum	493.00			44.00	18.00
Number of Time points or intervals (Excluding Zero)					7
Difference Factor - F1 [Acceptance Criteria : 0 - 15]					3.65
Similarity Factor - F2 [Acceptance Criteria : 50 - 100]					78.44

CONCLUSION: The main goal of this work was to develop Floating Effervescent tablets of Ranitidine Hydrochloride. The formulation design was expected to provide sustained release of Ranitidine Hydrochloride from the dosage form to treat for peptic and duodenal ulcers. Total 14 formulations were prepared using HPMCK100M, HPMCK4M, Guargum, Xanthum gum and were evaluated for various parameters. According to work plan the prepared tablets were evaluated for Hardness, Thickness, Friability, Invitro Buoyancy, Swelling Index, Dissolution profile, Weight, Drug content.

As formulations (F1-F4) show undesired release profiles, so drug: polymer ratio changed to 1:1 by decreasing the ratio of Mannitol and weight adjusted to 400mg. Formulations (F5-F8) showed better release profile as that of (F1-F4).

Formulations (F9-F14) are taken in combination of polymers. These set of formulations shows prolonged when compared to (F1-F8). Formulation (F9) shows desired drug release for 12 hours due to the combination of polymers HPMC K100M and Guar gum.

From results it was observed that the In vitro dissolution profile of Sustained release matrix tablets containing Ranitidine hydrochloride from the formulation F9, drug release at 0, 0.25, 0.5, 1, 2, 4, 6, 8, 10, 12hr was found to be 13.72%, 23.72%, 36.23%, 45.36%, 58.96%, 72.53%, 85.16%, 92.16 and 99.8% respectively.

The floating effervescent tablets of Ranitidine Hydrochloride 150mg provided sustained drug release for 12h. From the results it was observed that the F9 formulation of Ranitidine Hydrochloride using Guar gum and HPMC K100M as polymers was found to be the best formulation. Future scope was supposed to have pilot plant scale up, *in-vivo* evaluation and also industrial application of floating effervescent tablets of Ranitidine Hydrochloride.

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